

23th SSIP Summer School on Image Processing
14 July, 2015, Szeged, Hungary

Continuous and Discrete Image Reconstruction



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Steps of Machine Vision

- Image acquisition
- Preprocessing
- Segmentation
- Feature extraction
- Classification, interpretation
- Actuation

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Image Acquisition

by visible light



by X-rays



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X-rays

- 1895 - Wilhelm Conrad Röntgen describes the properties of X-rays
- Kind of electromagnetic radiation (similar to light but having more energy)
- Attenuation of X-rays depends on tissue → „Shadow” of the object from one direction



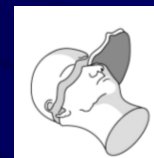
X-rays are Useful in Radiology (in some cases)



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Tomography

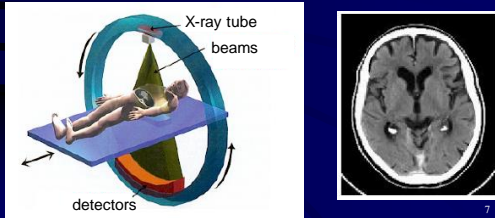
Tomos = part, section
Grapho = to write
Tomos + Grapho ≈ imaging by cross-sections (slices)



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Computerized Tomography

- A technique for imaging the 2D cross-sections of 3D objects (human organs) without seriously damaging them
- Take X-ray images from many angles and combine them in a clever way

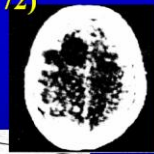


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The first CT (1972)



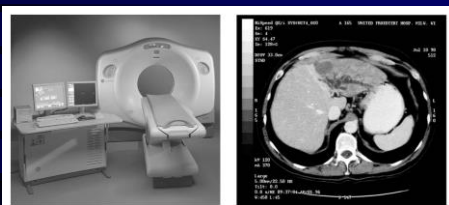
Godfrey N. Hounsfield
Nobel-prize 1979



Slide: Atila Kuba

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A Modern CT Scanner



Scanner

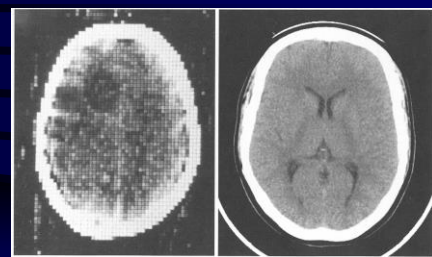
CT image

Figure 1.2

Medical Imaging Signals and Systems, by Jerry L. Prince and Jonathan Links.
ISBN 0-13-065353-5. © 2006 Pearson Education, Inc., Upper Saddle River, NJ. All rights reserved.

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Image Quality: Then and Now



first CT scanners

modern CT scanners

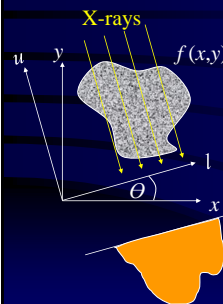
10

... or Even ...

... on-line scanning of how a fly tries to fly

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The Mathematics of CT

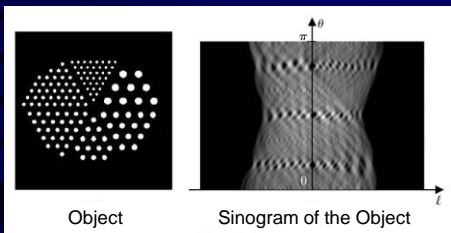


Reconstruct $f(x,y)$ from its projections where a projection in direction u (defined by angle θ) can be obtained by calculating the line integrals along each line parallel to u .

$$g(l, \theta) = \int_{-\infty}^{\infty} f(l \cos \theta - u \sin \theta, l \sin \theta + u \cos \theta) du$$

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Sinogram

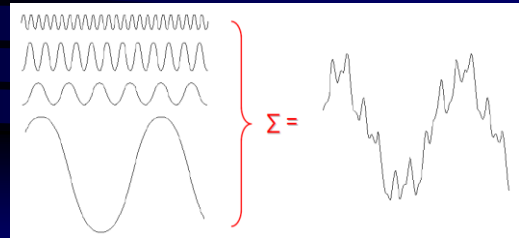


Sinogram: image of $g(l, \theta)$ with l and θ as rectilinear coordinates
 Reconstruction: sinogram \rightarrow image

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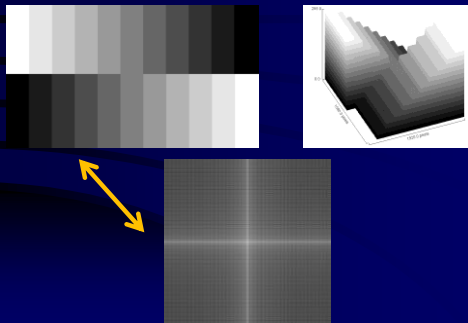
1D Fourier Transform

decompose a function into its sine and cosine components



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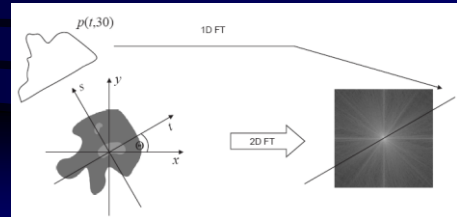
2D Fourier Transform



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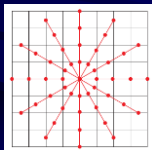
Projection-Slice Theorem

The 1D Fourier-transform of the projection taken from angle θ describes the values of the 2D Fourier-transform of the original image along a line passing through the origo with angle θ .



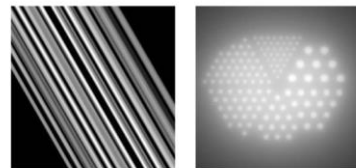
Fourier Reconstruction Method

- Take the 1D FT of all the projections
- Place them into the proper position in the frequency-domain
- Take the inverse 2D FT of the result



- Sampling, interpolation, inverse 2D FT

Backprojection Summation Image (laminogram)



One backprojection image Backprojection summation image (blur!)

Medical Imaging Signals and Systems, by Jerry L. Prince and Jonathan Links.
 ISBN 0-13-065353-5. © 2006 Pearson Education, Inc., Upper Saddle River, NJ. All rights reserved.

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Filtered Backprojection

- High frequencies (small details + noise) are undersampled \rightarrow blur
- Give higher weights to higher frequencies

Slide: Alexander L.C. Kwan

Filtered Backprojection with 240 Projections

An FBP Movie

- [Movie](http://hendrix.ei.dtu.dk/movies/moviehome.html) showing the FBP reconstruction process
 - 2D sinogram (projections)
 - high pass filtered for all angles
 - sinogram is backprojected into the image domain.
- Source: <http://hendrix.ei.dtu.dk/movies/moviehome.html>

ART – Algebraic Reconstruction Technique

- The interaction of the projection rays and the image pixels can be written as a system of equations
- Direct inverse methods are not applicable:
 - big system
 - underdetermined ($\#equations \ll \#unknowns$)
 - possibly no solution (if there is noise)
- Solve it iteratively satisfying just one projection in each step

An Example

(a)

An Example

$a+b=12$
 $c+d=8$

(a) (b)

An Example

$a+c=11$
 $b+d=9$

(a) (b) (c)

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An Example

$a+d=5$
 $b+c=15$

(a) (b) (c) (d)

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Discrete/Binary Tomography

- FBP and ART need several hundreds of projections
 - time consuming
 - expensive
 - may damage the object
 - not possible
- In certain applications the range of the function to be reconstructed is discrete and known → DT (only few (2-10) projections are needed)
- Binary Tomography: the range of the function is $\{0,1\}$ (absence or presence of material)

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KNOWING THE DISCRETE RANGE

# projs.	Conv. method	Discretized image	DT method
8			
12			
16			

I. Runkó, A.K., Z. Kiss, I. Rodek, 2003
Source: Attila Kuba

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Binary Reconstruction from 2 Projections

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Binary Reconstruction from 2 Projections

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Nonograms

Example for Uniqueness

3			
2			
1			
	3	2	1

3	1	1	1
2			
1			
	3	2	1

3	1	1	1
2			
1			
	3	2	1

3	1	1	1
2			
1			
	3	2	1

unique

Example for Inconsistency

3			
3			
1			
	3	3	1

3	1	1	1
3			
1			
	3	3	1

3	1	1	1
3	1	1	1
1			
	3	3	1

inconsistent

Classification

3			
3			
1			
	3	3	1

3	1	1	1
2	1	1	
1	1		
	3	2	1

1	1		
1		1	
	1	1	

1		1	
1		1	
	1	1	

inconsistent unique non-unique

Two Main Problems

Reconstruction: Construct a discrete set from its projections.

Uniqueness: Is a discrete set uniquely determined by a given set of projections?

Reconstruction

Ryser, 1957 – from row sums R and column sums S

Order the elements of S in a non-increasing way by $\pi \rightarrow S'$

Fill the rows from left to right $\rightarrow B$ (canonical matrix)

Shift elements from the rightmost columns of B to the columns where $S(B) < S'$

Reorder the columns by applying the inverse of π

R

2					
4					
3					
4					
1					

 S

3	4	3	2	1	1
---	---	---	---	---	---

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R

2					
4					
3					
4					
1					

 S

3	4	3	2	1	1
---	---	---	---	---	---

38

R

2					
4					
3					
4					
1					

 S

3	4	3	2	1	1
---	---	---	---	---	---

39

R

2					
4					
3					
4					
1					

 S

3	4	3	2	1	1
---	---	---	---	---	---

R

2	1	1			
4	1	1	1		
3	1	1	1		
4	1	1	1		
1					

 $S(B)$

5	4	3	2	0	0
4	3	3	2	1	1

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R

2					
4					
3					
4					
1					

 S

3	4	3	2	1	1
---	---	---	---	---	---

R

2	1	1			
4	1	1	1		
3	1	1	1		
4	1	1	1		
1					

 $S(B)$

5	4	3	2	0	0
4	3	3	2	1	1

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R

2					
4					
3					
4					
1					

 S

3	4	3	2	1	1
---	---	---	---	---	---

R

2	1	1			
4	1	1	1		
3	1	1	1		
4	1	1	1		
1					

 $S(B)$

5	4	3	2	0	0
4	3	3	2	1	1

R

2	1	1			
4	1	1	1		1
3	1	1	1		
4	1	1	1		
1					

 $S(B)$

5	4	3	1	0	1
4	3	3	2	1	1

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R

2							
4							
3							
4							
1							

 S

2							
4							
3							
4							
1							

 S'

R

2	1	1					
4	1	1	1	1			
3	1	1	1				
4	1	1	1	1			
1	1						

 $S(B)$
 $=B$

2	1	1					
4	1	1	1				1
3	1	1	1				
4	1	1	1	1			
1	1						

 $S(B)$

S'

4	3	3	2	1	1		
4	3	3	2	1	1		

 S'

5	4	3	2	0	1	1	
4	3	3	2	1	1		

 S'

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R

2	1	1					
4	1	1	1				1
3	1	1	1				
4	1	1	1			1	
1	1						

 $S(B)$

S'

5	4	3	0	1	1		
4	3	3	2	1	1		

 S'

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R

2	1	1					
4	1	1	1				1
3	1	1	1				
4	1	1	1			1	
1	1						

 $S(B)$

S'

5	4	3	0	1	1		
4	3	3	2	1	1		

 S'

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R

2	1	1					
4	1	1	1				1
3	1	1	1				
4	1	1	1			1	
1	1						

 $S(B)$

S'

5	4	3	0	1	1		
4	3	3	2	1	1		

 S'

5	4	1	2	1	1		
4	3	3	2	1	1		

 S'

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R

2	1	1					
4	1	1	1				1
3	1	1	1				
4	1	1	1			1	
1	1						

 $S(B)$

S'

5	4	3	0	1	1		
4	3	3	2	1	1		

 S'

5	4	1	2	1	1		
4	3	3	2	1	1		

 S'

R

2	1	1					
4	1	1	1			1	1
3	1	1	1				
4	1	1	1			1	
1	1						

 $S(B)$

S'

5	4	1	2	1	1		
4	3	3	2	1	1		

 S'

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R

2	1	1					
4	1	1	1				1
3	1	1	1				
4	1	1	1			1	
1	1						

 $S(B)$

S'

5	4	3	0	1	1		
4	3	3	2	1	1		

 S'

5	4	1	2	1	1		
4	3	3	2	1	1		

 S'

R

2	1	1					
4	1	1	1			1	1
3	1	1	1				
4	1	1	1			1	
1	1						

 $S(B)$

S'

5	4	1	2	1	1		
4	3	3	2	1	1		

 S'

5	2	3	2	1	1		
4	3	3	2	1	1		

 S'

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Uniqueness and Switching Components

configuration

The presence of a switching component is necessary and sufficient for non-uniqueness

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Ambiguity

Due to the presence of switching components there can be many solutions with the same two (or even more) projections

Use prior information (convexity, smoothness, etc.) of the binary image to be reconstructed

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Structural Priors

pebble beds metal-, plastic foams
cracks air bubbles, metal alloy defects

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Reconstruction as Optimization

$$\begin{cases}
 x_1 + x_2 = 2 \\
 x_3 + x_4 = 2 \\
 x_1 + x_3 + x_5 = 2 \\
 x_2 + x_4 + x_6 = 3
 \end{cases}
 \quad b$$

$$P = \begin{pmatrix} 1 & 1 & & & & \\ & & 1 & 1 & & \\ 1 & & & & 1 & 1 \\ & & & & & & 1 & 1 & 1 \end{pmatrix}
 \quad x = \begin{pmatrix} x_1 \\ x_2 \\ x_3 \\ x_4 \\ x_5 \\ x_6 \end{pmatrix}$$

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Optimization

$Px = b \quad x \in \{0,1\}^{m \times n}$

Problems:

- binary variables
- big system
- underdetermined (#equations << #unknowns)
- possibly no solution (if there is noise)

$C(x) = \|Px - b\|^2 + g(x) \rightarrow \min$

Term for prior information: structure, similarity to a model image, etc.

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Neighbouring Slices

Subsequent slices are similar

previous slice

1	1	1	
1	1	1	1
	1	1	

→

cost matrix

8	7	6	7	8	9
7	4	3	4	5	8
7	4	2	2	4	7
9	8	4	4	5	8
9	9	7	7	8	9

$x \in \{0,1\}^{m \times n}$

$$C(x) = \|Px - b\|^2 + \sum_{i,j} c_{ij} x_{ij} \rightarrow \min$$

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Solving the Optimization Task

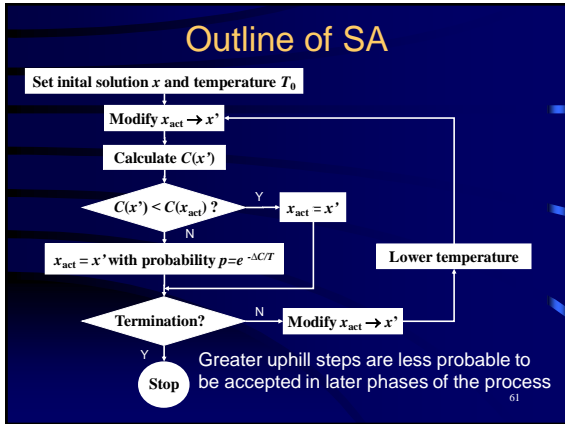
- **Problem:** Classical hill-climbing algorithms can become trapped in local minima.
- **Idea:** Allow some changes that increase the objective function.

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Simulated Annealing

- **Annealing:** a thermodynamical process in which a metal cools and freezes.
- Due to the thermal noise the energy of the liquid in some cases grows during the annealing.
- By carefully controlling the cooling temperature the fluid freezes into a minimum energy crystalline.
- **Simulated annealing:** a random-search technique based on the above observation.

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Finding the Optimum

- Tuning the parameters appropriately SA finds the global optimum
- Fine-tuning of the parameters for a given optimization problem can be rather delicate

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SA in Pixel Based Reconstruction

- A binary matrix describes the binary image
- Randomly invert matrix value(s)

$$\begin{bmatrix} 0 & 1 & 1 & 1 & 0 \\ 1 & 1 & 1 & 1 & 0 \\ 0 & 0 & 0 & 0 & 0 \\ 1 & 1 & 1 & 0 & 1 \end{bmatrix} \rightarrow \begin{bmatrix} 0 & 1 & 1 & 1 & 1 \\ 1 & 1 & 1 & 1 & 0 \\ 0 & 0 & 0 & 0 & 0 \\ 1 & 1 & 1 & 0 & 0 \end{bmatrix}$$

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SA in Geometry Based Reconstruction

- The binary image is described by parameters of geometrical objects, e.g. (x,y,r)
- Randomly modify parameter(s) of object(s)

[[16,53,17],(44,35,25),(26,13,12),(43,8,12)] + [[13,50,23]]

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Modifying Parameters

Operation	Parameters
Delete	(x ₁ , y ₁ , r ₁) (x ₂ , y ₂ , r ₂) (x ₃ , y ₃ , r ₃) (x ₄ , y ₄ , r ₄) (x₁, y₁, r₁)
Add	(x ₁ , y ₁ , r ₁) (x ₂ , y ₂ , r ₂) (x ₃ , y ₃ , r ₃) (x ₄ , y ₄ , r ₄) (x ₅ , y ₅ , r ₅) (x ₆ , y ₆ , r ₆) (x₁, y₁, r₁)
Move	(x ₁ , y ₁ , r ₁) (x ₂ , y ₂ , r ₂) (x ₃ , y ₃ , r ₃) (x ₄ , y ₄ , r ₄) (x ₅ , y ₅ , r ₅) (x ₆ , y ₆ , r ₆) (x₁, y₁, r₁)
Resize	(x ₁ , y ₁ , r ₁) (x ₂ , y ₂ , r ₂) (x ₃ , y ₃ , r ₃) (x ₄ , y ₄ , r ₄) (x ₅ , y ₅ , r ₅) (x ₆ , y ₆ , r ₆) (x₁, y₁, r₁)

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Nondestructive Testing: Pipe Corrosion, Deposit, Crack, etc. Study

32 fan beam X-ray projections

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Results with and without Noise



no noise



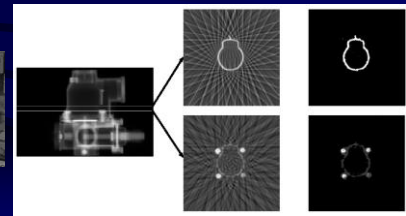
10 % Gaussian noise

Source: A. Nagy

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Neutron Tomography I.

- Gas pressure controller
 - 18 projections, pixel based, also multilevel



Source: A. Nagy

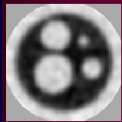
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Neutron Tomography II.

- Reconstruction of disks (air bubbles)
 - 4 projections, geometry based



FBP 60 proj.



DT 4 proj.



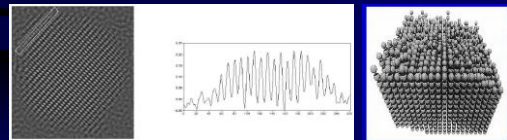
Source: L. Rodek

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Electron Microscopy

QUANTITEM: a method which provides quantitative information for the number of atoms lying in a single atomic column from HRTEM images

Possible to detect crystal defects (e.g. missing atoms)



Source: Batenburg, Palenstijn

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